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# Sensors and Actuators B: Chemical

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# Development of a nanocomposite chemiresistor sensor based on $\pi$ conjugated azo polymer and graphene blend for detection of dissolved oxygen



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#### ARTICLE INFO

Keywords: Azo conductive polymers Chemiresistor Nanocomposite Oxygen sensor Graphene

### ABSTRACT

The present paper describes the electrochemical impedance activity of a hybrid film with graphene and poly(azo-Bismarck Brown Y) as the chemiresistor material. This nanocomposite film exhibits interesting properties based on the redox properties of the azo polymer combined with the great electronic conductivity and stability of graphene. Electrochemical impedance spectroscopy at the poly(azo-BBY)-rGO electrode in solutions with different dissolved  $\rm O_2$  concentrations revealed that the resistance values are very sensitive to variations in the  $\rm O_2$  concentration.

#### 1. Introduction

Chemiresistors represent a new class and emerging area of electrochemical sensors [1,2]. Their operation is based on the change in the electrical resistance of the material due to chemical interaction with the analyte [3]. A variety of materials have been investigated for application as chemiresistors, such as semiconductor metal oxides [4], conductive polymers [5], organic semiconductors [6] and carbon-based materials [7,8]. Most chemiresistors are developed for gas sensing [8–10], with a few works dedicated to the sensing of chemical species in electrolyte solutions [11,12].

Composite materials classically combine two or more materials to take advantage of the best properties and characteristics of each [13]. Polymer-graphene nanocomposites prepared by combining the vast  $\pi$ -conjugated system of conducting polymers with the various properties of graphene have been highlighted [14–16]. In the case of azo conductive polymers (azo polymer), in addition to the advantages of being a conductive polymer, it still has the advantage of the presence of redox active sites due to the inclusion of diazonium groups in the polymer [17].

Here, we investigate the charge transfer of poly(azo-Bismark Brown Y) with rGO (poly(azo-BBY)-rGO) in the presence of different concentrations of molecular oxygen with the objective of constructing a chemiresistor sensor for monitoring dissolved oxygen in aqueous solution.

All measurements were performed in a conventional electrochemical cell containing three electrodes: a saturated calomel electrode (SCE) as the reference; platinum wire as the counter electrode and a fluoride-doped tin oxide (FTO) electrode coated with a poly(azo-BBY)-rGO blend as the working electrode  $(1.0\,\mathrm{cm}^2)$ . All electrochemical measurements were performed with Palsens3 interfaced PSTrace 5.2 software. All reagents used were of high purity  $\geq 98\%$  (Sigma Aldrich).

The poly(azo-BBY)-rGO sensor material was prepared on the FTO surface by potential cycling between -0.30 and +1.00 V (vs. SCE) for 20-cycle scans at a scan rate of  $10\,\mathrm{mV\,s^{-1}}$  in a deaerated solution containing  $10\,\mathrm{mmol\,L^{-1}}$  BBY and a  $1.00\,\mathrm{mg\,mL^{-1}}$  suspension of graphene oxide (Sigma Aldrich) in a  $0.1\,\mathrm{mol\,L^{-1}}$  HCl medium.

The charge transfer resistance of the polymer composite with molecular oxygen in a solution of  $0.5\,\mathrm{mol}\,L^{-1}$  KCl (pH 2.0) and  $0.05\,\mathrm{mol}\,L^{-1}$  phosphate buffer (pH 7.4) was investigated using EIS measurements at an applied potential of  $-0.30\,\mathrm{V}$  (vs. SCE). The pH solutions were adjusted with hydrochloridric acid and sodium hydroxide.

The EIS measurements were performed through the incidence of a sine wave of  $10\,\text{mV}$  applied in a frequency range of  $50\,\text{kHz}$  to  $0.1\,\text{Hz}$  with  $10\,\text{step/dec}$ . All spectra were recorded at  $25\,^{\circ}\text{C}$ . The analysis of the complex plane impedance spectra was determined by ZPlot 2.4 software. The determination of dissolved oxygen was performed after the addition of an aliquot of a  $Na_2SO_3$  standard solution ( $0.1\,\text{mol}\,\text{L}^{-1}$ ). The

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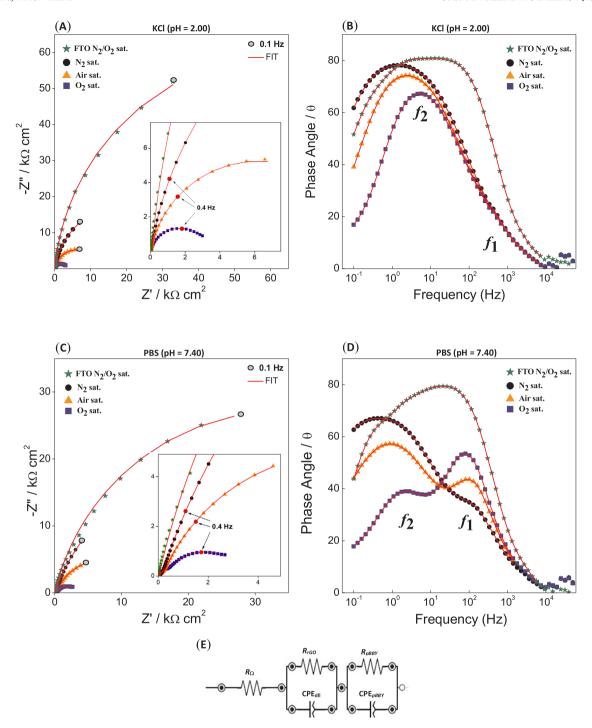


Fig. 1. (A) Nyquist and (B) Bode impedance diagrams at unmodified FTO ( $\star$ ) and poly(azo-BBY)-rGO/FTO in solutions of KCl (pH 2.0) saturated with N<sub>2</sub> ( $\bullet$ ), air ( $\wedge$ ), and O<sub>2</sub> ( $\blacksquare$ ). Applied potential of -0.30 V vs. SCE. (C) Nyquist and (D) Bode impedance diagrams at unmodified FTO ( $\star$ ) and poly(azo-BBY)-rGO/FTO in PBS (pH 7.4) saturated with N<sub>2</sub> ( $\bullet$ ), air ( $\wedge$ ), and O<sub>2</sub> ( $\blacksquare$ ). Applied potential of -0.30 V vs. SCE. (E) Electrical equivalent circuit used to fit the complex plane impedance spectra at poly(azo-BBY)-rGO/FTO.

gas concentration was calculated from the chemical reaction of oxygen consumption by sulfite.

# 3. Results and discussion

#### 3.1. Performance of the sensing platform

The poly(azo-BBY)-rGO film was studied by EIS, which provided important information about the physical and interfacial properties of the sensing platform. Fig. 1 show the typical impedance datas (Nyquist

and Bode) obtained at the composite electrode in KCl (pH 2.0) and PBS (pH 7.4) in the absence of oxygen and in the presence of normal and saturated oxygen levels. To analyze the characteristics of the impedance plot, an equivalent circuit (Fig. 1E) composed of a cell resistance ( $R_{\Omega}$ ) in series with two parallel R CPE combinations was used to fit the spectra. The first R CPE combination is associated with the solution/rGO interface ( $R_{pGO}$  and CPE $_{dl}$ ), while the second R CPE combination is attributed with the rGO/polymer interface ( $R_{pBBY}$  and CPE $_{pBBY}$ ), and their values (Table 1) depend on the oxygen content and pH of the aqueous solution.

Table 1
Parameters determined from fitting the electrochemical impedance spectra of the composite electrode for solutions with different dissolved oxygen conditions to the equivalent circuit shown in Fig. 1E. The errors presented for the fit were below 2%.

	$R_{\Omega}$	$R_{rGO}$ (k $\Omega$ cm <sup>2</sup> )	$R_{pBBY}$	$\frac{\text{CPE}_{dl}}{(\text{mF cm}^{-2}  \text{s}^{\alpha - 1})}$	$lpha_{dl}$	$CPE_{pBBY}$ $(mF cm^{-2} s^{\alpha-1})$	$lpha_{pBBY}$
KCl (pH = 2.00)	)						
N <sub>2</sub> sat.	0.025	0.021	41.6	0.486	0.691	0.0937	0.901
Air sat.	0.025	0.020	12.3	0.348	0.735	0.111	0.898
O <sub>2</sub> sat.	0.026	0.016	3.29	0.237	0.780	0.121	0.879
PBS (pH = $7.40$	)						
N <sub>2</sub> sat.	0.047	0.085	49.6	0.160	0.800	0.103	0.790
Air sat.	0.047	0.131	14.6	0.170	0.759	0.0380	0.922
$O_2$ sat.	0.046	3.050	2.55	0.022	0.999	0.180	0.721

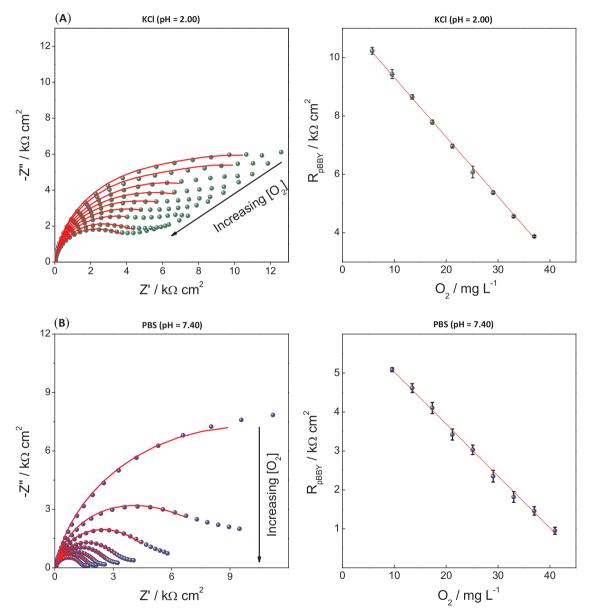


Fig. 2. Impedance spectra of the chemiresistor material with different concentrations of dissolved oxygen in solutions of (A) KCl (pH 2.0) and (B) PBS (pH 7.4) with their respective calibration curves. The error bars represent the standard deviation from three separate experiments using the same sensor.

In the Bode plots (Fig. 1B and D), the resistive and capacitive regions are clearly distinguished together with the information provided by the frequency dependence of the phase angle  $(\theta)$ , which is a very sensitive indicator of small changes in such spectra [18]. As shown in Fig. 1B and D, it is possible to verify the presence of two constant phase

elements (CPE) due to the presence of two phase angles located in the high-medium  $(f_1)$  and medium-low  $(f_2)$  frequency regions for both studied electrolytes [19]. It is clearly seen that in the acidic medium, the phase angles  $(f_1)$  attributed to the solution/rGO interface were practically constant and that the polymer became more conductive in

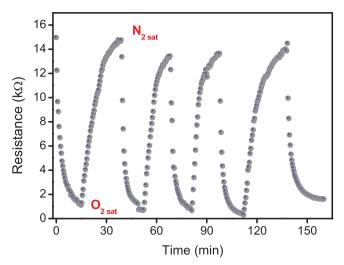


Fig. 3. Response of the poly(azo-BBY)-rGO film sensor as a function of time in KCl (pH 2.0) at a fixed frequency of 0.1 Hz. Applied potential =  $-0.30\,\text{V}$  vs. SCE.

the presence of molecular oxygen. At negative potentials, poly(azo-BBY) is in its reduced form (Eq. (1)) and can supply protons and electrons to the dissolved oxygen molecules.

The decrease in the resistance results from the reaction between molecular oxygen and the hydrazine groups present in the polymer [17,20]. The electronic conductivity of the polymer is due to the  $\pi$ -conjugation present in the polymer chains [21].

In PBS (Fig. 1D), contrary to the observed phase angle for the polymer, the presence of molecular oxygen increased the phase angle for the solution/rGO interface. From the EIS analysis (see Table 1), it is clear that the graphene on the film surface became more porous, and the resistance increased at the interface in the phosphate medium (slightly alkaline). This result can be attributed to the microoxidation of the graphene by molecular oxygen [22]. Padey and collaborators [23] reported that molecular oxygen could chemically adsorb on the graphene defects, and the oxidation process led to the formation of pits in the graphene. However, a more detailed study on the effect of the pH will be given later in a new work. Even so, the impedance related to the rGO/polymer interface decreased with variations in the dissolved oxygen concentration for low and medium frequencies. To confirm the recognition of dissolved O2 by the poly(azo-BBY) film, impedance spectra at an unmodified FTO electrode in solutions saturated with molecular oxygen and molecular nitrogen were recorded at  $-0.30 \,\mathrm{V}$  for both studied electrolytes (insert in Fig. 1A and C). There was no change in the spectral profile, indicating that at -0.30 V, there was no molecular oxygen reduction at the electrode surface.

# 3.2. Chemiresistor response to dissolved oxygen

The impedance response of the poly(azo-BBY)-rGO film to different concentrations of dissolved oxygen was examined in a KCl solution (pH 2.0) and a PBS solution (pH 7.4) at frequencies from 50 kHz to 0.1 Hz at an applied potential of  $-0.30\,\mathrm{V}$  (vs. SCE). The Nyquist impedance diagrams recorded at the chemiresistor material with different

dissolved  $O_2$  concentrations in KCl and PBS media are shown in Fig. 2A and B, respectively.

The respective linear relationships between the resistance and  $O_2$  concentration in the range of  $5.75\,\text{mg}\,\text{L}^{-1}$  (0.018 mmol  $\text{L}^{-1}$ ) to  $40.9\,\text{mg}\,\text{L}^{-1}$  (1.28 mmol  $\text{L}^{-1}$ ) were represented by Eq. (3) and Eq. (4):

$$R_{\rm pBBY}~({\rm k}\Omega~{\rm cm}^2)=11.3\pm0.06-0.204\pm0.003~[{\rm O}_2~({\rm mg\,L}^{-1})]~({\rm n}=9;{\rm R}^2=0.9989)~{\rm for~KCl}~({\rm pH~2.0})$$
 (3)

$$R_{\rm pBBY}~({\rm k}\Omega~{\rm cm}^2) = 6.36 \pm 0.04 - 0.133 \pm 0.002~[{\rm O}_2~({\rm mg\,L}^{-1})]~({\rm n} = 9; {\rm R}^2 = 0.9985)~{\rm for~PBS}~({\rm pH~7.4})$$
 (4)

For the chemiresistor response, the decrease in the resistance ( $R_{pBBY}$ ) with increasing amount of  $O_2$  is related to an increase in the amount of charge transferred between the polymer and molecular oxygen. The impedance dynamic response of the poly(azo-BBY)-rGO/FTO sensor (Fig. 3) was examined in KCl solutions saturated with  $O_2$  and  $N_2$ , with the frequency fixed at 0.1 Hz. The sensor exhibited good repeatability with a relative variation of 4.1% in the overall response of the chemiresistor per regeneration cycle.

# 4. Conclusion

The poly(azo-BBY)-rGO film exhibits a good  $O_2$  recognition ability in both acidic solution and slightly alkaline solution due to the high affinity of the hydrazine group with molecular oxygen. The resistance at the poly(azo-BBY)-rGO/FTO film increases linearly with decreasing amount of dissolved  $O_2$  in the electrolyte solution. Two calibration curves were developed, revealing sensitivities of 0.204 k $\Omega$  cm<sup>2</sup> L mg<sup>-1</sup> and 0.133 k $\Omega$  cm<sup>2</sup> L mg<sup>-1</sup> for  $O_2$  detection at pH 2.00 and pH 7.40, respectively. This chemiresistor material will be adapted for the measurement of mitochondrial oxygen consumption.

#### Acknowledgments

The authors acknowledge FAPESP (2016/09017-1) for financial support. A.O.O. thanks CAPES-Brazil for a master fellowship. SJT  $\div$ 

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